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Differentiation of multiple adrenal adenoma subtypes based on a radiomics and clinicoradiological model: a dual-center study

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Abstract

Background The prevalence and detection rates of adrenal incidentalomas have been on the rise globally, with more than 90% of these lesions pathologically classified as adrenocortical adenomas. Among these, approximately 30% of patients present with hormone-secreting adenomas, leading to the deterioration of their health, with some requiring surgical resection. The available methods for adrenal function evaluation are invasive and costly. Moreover, their accuracy is influenced by numerous factors. Therefore, it is imperative to develop non-invasive and simplified preoperative diagnostic approach.

Methods A retrospective study was performed on 169 patients from two tertiary medical centers. Subsequently, radiomics features were extracted after tumor margins were delineated layer-by-layer using a semi-automatic contouring approach. Feature selection was achieved in two cycles, with the first round utilizing a support vector machine (SVM) and the second round using a LASSO-based recursive feature elimination algorithm. Finally, logistic regression models were constructed using the clinico-radiological, radiomics, and a combination of both.

Results After a comprehensive evaluation of the predictive indicators, the logistic regression classifier model based on the combined clinico-radiological and radiomic features had an AUC of (0.945, 0.927, 0.856) for aldosterone-producing adenoma (APA), (0.963, 0.889, 0.887) for cortisol-producing adenoma (CPA), and (0.940, 0.765, 0.816) for non-functioning adrenal adenoma (NAA) in the training set, validation set, and external test set, respectively. This model exhibited superior predictive performance in differentiating between the three adrenal adenoma subtypes.

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Conclusions A logistic regression model was constructed using radiomics and clinico-radiological features derived from multi-phase enhanced CT images and conducted external validation. The combined model showed good overall performance, highlighting the feasibility of applying the model for preoperative differentiation and prediction of various types of ACA.

Keywords Adrenocortical adenomas, Radiomics, Computed tomography, Prediction model

Introduction

Adrenal incidentaloma (AI) refers to adrenal nodules discovered during imaging examinations conducted for health check-ups or non-adrenal diseases, with a maximum diameter ≥ 1 cm. Therefore, AI is an imaging-based definition, presenting with pathological changes, including tumors, nodular hyperplasia, cysts, or inflammatory nodules, among others. As the utility of medical imaging examinations increases and people's awareness about the need for health check-ups increases, the incidence and detection rate of AI have been increasing globally [1–4]. In most cases, AI originates in the adrenal cortex, with over 90% pathologically classified as adrenocortical adenomas (ACA), among which nearly 30% exhibit clinical symptoms [5, 6]. These include aldosterone-producing adenomas (APA), which are associated with hypertension and hypokalemia, and cortisol-producing adenomas (CPA), manifesting as hypertension, moon face, buffalo hump, and central obesity, collectively referred to as functioning AI with potentially serious detrimental effects on the patients. Non-functioning adrenal adenomas (NAA) without clinical symptoms can be managed through observation, whereas adrenal adenomas with hormone secretion functions require surgical intervention [7].

It has been found that the assessment of adrenal adenoma functionality solely based on radiological examinations may not accurately distinguish all types of conditions [8–10]. Although various auxiliary diagnostic methods such as the aldosterone/renin ratio (ARR), captopril test, seated saline infusion test, oral sodium loading test, 1 mg dexamethasone suppression test, and adrenal vein sampling have been developed to differentiate functional from non-functional adrenal adenoma [11], their performance is limited by several factors including, reference values, healthcare center conditions, test errors, patient physiological conditions or economic factors, and result turnaround time.

Computed tomography (CT) is routinely applied in preoperative examination of patients with adrenal masses is currently the preferred method for preoperative localization and qualitative diagnosis of adrenal tumors. According to the updated 2017 American College of Radiology (ACR) white paper and the latest guidelines from the European Society of Endocrinology/European Network for the Study of Adrenal Tumors, incidental adrenal tumors should first undergo non-enhanced CT imaging to determine their CT attenuation values. A threshold of 10 HU is generally selected, where lesions with attenuation values below 10 HU are generally considered benign. For those with values greater than 10 HU, further enhanced CT scans are needed to facilitate classification [12, 13]. Evidence from prior studies has demonstrated that attenuation values may be influenced by equipment parameters such as kVp, which reduce the diagnostic accuracy for adrenal tumors [14]. Moreover, the accuracy of CT is highly dependent on the diagnostic expertise of radiologists, and it cannot accurately differentiate the subtypes of adrenal cortical adenomas. Radiomics provides valuable evidence for early tumor diagnosis, differentiation, clinical decision-making, and prognosis prediction in a convenient and non-invasive manner, surpassing traditional imaging techniques in these aspects.

In this study, we applied CT radiomics methods, as well as preoperative adrenal function tests and postoperative pathological diagnosis, to facilitate ACA classification. Radiomic single-phase models (including unenhanced, arterial, and venous phase models), a triphaic model, a clinico-radiological model, and a clinico-radiologicalradiomics model (combine model) were constructed using abdominal enhanced CT images from the unenhanced, arterial, and venous phases, along with the clinico-radiological data. The performance of the six models was compared using metrics such as Receiver Operating Characteristic curve (ROC), Area Under the Curve (AUC), sensitivity, and accuracy. The aim of the study was to predict different types of ACA using a more objective and non-invasive approach, thereby providing data to guide clinical decision-making, help clinicians select appropriate diagnostic and treatment options, and assess the prognosis.

Materials and methods

This retrospective study was approved by the Medical Ethics Committee of the First People's Hospital of Yunnan Province (No. KHLL2023-KY170) and the Second Affiliated Hospital of Kunming Medical University (No. 2023-233). Given the retrospective nature of the study and use of deidentified data, the ethics committee waived the requirement for informed consent. Tumor segmentation, feature extraction, preprocessing, screening, and classifier model construction were performed on the Darwin Intelligent Medical Research Platform (details and relevant agreements can be found at https://arxiv.org /abs/2009.00908).

Patient selection

Patients who underwent adrenalectomy for adrenal masses and had definitive pathological diagnoses, were treated in the Urology Department of the First People's Hospital of Yunnan Province (Center One) from January 2016 to June 2023, as well as in the Urology Department of the Second Affiliated Hospital of Kunming Medical University (Center Two) from January 2021 to May 2023, were enrolled in the study. Using the aforementioned criteria, 414 and 669 patients were respectively analyzed. The following inclusion criteria were used: (1) Patients who underwent adrenalectomy for adrenal masses and had definitive pathological diagnoses. (2) Patients who underwent abdominal contrast-enhanced CT imaging within one month before treatment and obtained multiphase (unenhanced, arterial and venous) images. The exclusion criteria were: (1) Patients not falling under the pathological classification of interest. (2) Those with adrenal masses with a diameter below 1 cm. (3) Patients with poor-quality CT images affecting the image segmentation due to artifacts. (4) Patients with incomplete clinical or imaging data, or those for whom the specific tumor subtype could not be determined. (5) Patients whose hormone levels might be influenced by medication intake.

After analyzing the postoperative pathological results and inclusion/exclusion criteria, 169 patients with ACA were enrolled, with 45 cases from Center One and 124 cases from Center Two. The patients' blood pressure status and adrenal function test results were also determined [15, 16] (Due to ethnic and regional differences, reference was made to the relevant guidelines and

Table 1 The diagnostic criteria for ACAs classification

Tumor types	Diagnostic criteria				
NAA	1.The pathological diagnosis is ACAs. 2.Non-functional (normal blood biochemistry markers associated with functional adenomas)				
CPA	 The pathological diagnosis is ACAs. The 24-hour serum cortisol level is greater than 113.35 mmol/L (4.1 μg/dL). The morning 8 a.m. adrenocorticotropic hormone (ACTH) level is less than 3.0 pmol/L (13.63 pg/mL). Clinical exclusion of other categories 				
APA	 1.The pathological diagnosis is ACAs. 2.History of hypertension and hypokalemia associated with APA. 3.ARR, based on renin activity: ARR > 30 (ng/dL) / (ng·mL⁻¹·h⁻¹); based on renin concentration: ARR > 37 (mU/L) / (nq/dL). 				

Note: NAA: Criteria 1 and 2 must be simultaneously fulfilled for diagnosis.CPA: Criteria 1, 2, 3, and 4 must be simultaneously fulfilled for diagnosis.APA: Criteria 1, 2, and 3 must be simultaneously fulfilled for diagnosis. Explanation: NAA: non-functioning adrenal adenoma. CPA: Cortisol-producing adenoma. APA: Aldosterone-producing adenoma

recommendations for adrenal diseases in China. The specific details are presented in Table 1), the 169 adrenal adenoma patients were classified into APA (n = 15/n = 41), CPA (n = 15/n = 34), and clinically NAA (n = 15/n = 49) groups. Subsequently, three predictive models were constructed: APA versus other ACA, CPA versus other ACA, and clinically non-functional adenoma versus other ACA. The data from Center Two served as the internal cohort for the training and validation cohorts (at an 8:2 ratio), while the data from Center One served as an external cohort for testing. Patients' inclusion and exclusion criteria are depicted in Fig. 1.

Collection of clinical and routine imaging parameters

The collected clinical parameters of patients included age, sex, tumor laterality, and maximum tumor diameter. Routine imaging parameters included the mean attenuation value, maximum attenuation value, minimum attenuation value, and standard deviation of the mean attenuation value in the unenhanced, venous, and arterial phases, as well as the differences between the mean attenuation values in the venous and arterial phases compared to the unenhanced phase. Besides age, sex, and laterality, all other features were measured using the values obtained from three consecutive transverse CT images of the tumor's maximum diameter. Each image was measured three times, ensuring that areas with cystic changes or calcification were excluded, and the final value was the average of these measurements.

CT image acquisition and processing

Several multi-slice CT scanners (Brilliance iCT, Philips; SOMATOM Force, SOMATOM Drive, or SOMATOM Perspective, Siemens; Aquilion ONE, Canon) were utilized to perform abdominal contrast-enhanced scanning. The collimation settings were 128×0.625 , 192×0.6 , $128 \times 0.6, 64 \times 0.6, and 100 \times 0.5$, with a tube voltage range of 80–120 kVp and a matrix size of 512×512 . The gantry rotation time was 0.5 s, with a pitch range of 0.5-0.993 and a slice thickness varying between 0.9 mm and 5 mm. For Brilliance iCT, the tube current was set at 200-250 mAs, while for the other scanners, it was automatically adjusted. Non-ionic contrast agents, Iohexol Injection or Iomeprol Injection, were administered via the cubital vein at a dosage of 450 mg I/kg, with concentrations of 350 mg I/ml for Iohexol and 400 mg I/ml for Iomeprol. Arterial phase imaging was performed using the threshold-triggering technology, while venous phase imaging was conducted with a fixed delay of 50-70 s. Detailed information on radiation exposure, such as CTDI and DLP [17] are shown in Table S1. At the end of CT scanning, the image data were transferred to the image workstation Picture Archiving and Communication System (PACS) for post-processing, and the data were saved in



Fig. 1 A flowchart showing the patient inclusion and exclusion process

the Digital imaging and communications in medicine format.

Region of interest segmentation and feature extraction

Semi-automatic segmentation was performed by a urologist with 7 years of experience in urinary system imaging using the Darwin Intelligent Medical Research Platform. To ensure objectivity, the urologist was blinded to all patient clinical information and carefully avoided including the tumor capsule, adrenal gland, and adjacent tissues within the regions of interest. After delineation, another urologist with 17 years of extensive experience in urinary system imaging examined each annotation individually. Any discrepancy between the two urologists was resolved through consultation by a urologist with over 20 years of urinary system imaging experience to determine the final region of interest. Subsequently, radiomic features were automatically extracted from each patient's images in the unenhance, arterial, and venous phases (The details of feature extraction methods can be obtained from https://arxiv.org/abs/2009.00908).

Feature selection and model construction

To validate the accuracy of tumor ROI delineation, we conducted Dice coefficient analysis and ICC analysis as detailed below:

Thirty patients from the internal cohort were randomly selected based on the classification ratios, and the regions of interest were segmented and features extracted by two urologists: one with 7 years of experience and the other with 17 years of experience in urological imaging. Firstly, the Dice coefficient was calculated from the ROIs delineated by the two experts. The calculation formula is presented below [18]:

$$Dice = \frac{2 \times |X \cap Y|}{|X| + |Y|}$$

Following confirmation of inter-reader reliability, the ICC was calculated using the method described by McGraw and Wong [19] for all features. Features with an ICC value exceeding 0.75 were considered robust and included in subsequent analyses.

$$\mathrm{ICC} = \frac{\mathrm{MS}_{\mathrm{R}} - \mathrm{MS}_{\mathrm{E}}}{\mathrm{MS}_{\mathrm{R}} + (\mathrm{k} - 1) \,\mathrm{MS}_{\mathrm{E}}} + \frac{\mathrm{k}}{\mathrm{n}} \times (\mathrm{MS}_{\mathrm{C}} - \mathrm{MS}_{\mathrm{E}})$$

Next, the "min-max normalization" method was applied to preprocess the features, whereby each feature dimension of all samples was linearly transformed to the range of (0,1). For each feature $X \in \mathbb{R}^{N \times d}$ where N is the total number of samples and d is the feature dimension. Minmax normalization was performed on each column feature $X \in \mathbb{R}^N$ as follows:

$$x_i {=} \frac{x_i {\text{-}} x_{\min}}{x_{\max} {\text{-}} x_{\min}}$$

where $1 \le i \le N$, and x_{max} and x_{min} are the maximum and minimum element values in x, respectively.

Subsequently, the SelectFromModel algorithm, with SVM as the evaluation model, was utilized to perform the first round of screening for radiomic features.: unenhanced, arterial, and venous phases. Subsequently,

feature selection was performed in the second round using the RFECV (Recursive Feature Elimination with Cross-Validation) algorithm (The RFECV algorithm assesses feature importance by iteratively removing the least important features after each training iteration. This process continues until the classification performance begins to decline or the minimum number of features is reached, based on the LASSO model, to obtain the final robust radiomics features. Triphasic radiomics features were generated by combining radiomic features extracted from unenhanced, arterial, and venous phase images. Subsequently, a logistic regression classification model was developed using these combined radiomics features. The selection of clinico-radiological features was based on inter-group comparisons using data from the training set. Features with statistical significance (P < 0.05)were enrolled in the final analysis. Separate models for clinico-radiological features were constructed and combined with the optimal radiomics model to establish a joint model. Finally, external data were utilized to test the generalizability of this model. The overall workflow of the radiomics analysis is presented in Fig. 2.

Statistical analysis

Statistical analysis was conducted using the SPSS 26.0 software. Categorical data were compared between the groups using Pearson's chi-square test. For continuous variables that followed a normal distribution and exhibited homogeneity of variances, one-way analysis of



Fig. 2 Radiomics analysis workflow diagram

variance (ANOVA) was applied. The results are expressed as the mean \pm standard deviation. For data that did not follow a normal distribution or exhibited heterogeneity of variances, as well as intergroup comparisons, the nonparametric Kruskal-Wallis H test was utilized, and the results were expressed as the median and interquartile range. A *P* < 0.05 was considered statistically significant.

The Receiver Operating Characteristic curve (ROC) analysis and its calculated Area Under the Curve (AUC), sensitivity, specificity, precision, and accuracy was employed to assess the predictive performance of the model. External data were employed for external testing to further evaluate the generalizability of the model.

Results

Comparison of clinico-radiological features among the three patient groups

A total of 169 patients were enrolled from two centers, with 45 cases from Center One and 124 cases from Center Two. Patients from Center Two were assigned to the internal data group with 99 cases in the training set (including 39 APA, 27 CPA, and 33 clinically non-functional adenomas) and 25 cases in the validation set (including 10 APA, 7 CPA, and 8 clinically non-functional

adenomas). Patients from Center One were designated as the external testing set (comprising 15 cases each of APA, CPA, and clinically non-functional adenomas). Although significant differences were observed between the three patient groups in baseline characteristics, including the standard deviation of attenuation values in the arterial phase, the standard deviation of attenuation values in the venous phase, and the difference in attenuation values between the venous phase and the unenhanced phase (Table 2). However, these three features were not significantly different in the subsequent three-class classification analysis of the training set (Table 3) and were not included in the final model.

Extraction of radiomic features and optimal feature selection

Table S2 presents the Dice similarity coefficients obtained from the analysis. A total of 5343 features were extracted, including 1781 features from each unenhanced, arterial, and venous phase images using an intelligent medical research platform. Following the ICC analysis, 4830 robust features (ICC > 0.75) with 1583 from the unenhanced, 1621 from the arterial, and 1626 from the venous. In the first round of feature selection for

Table 2 Analysis of clinical and conventional radiological features in the training, validation, and test sets

	Total(N = 169)	Training set(N = 99)	Validation set(N=25)	Test set(N=45)	χ²/H/F	P-value
Age, years	50(41,57)	51(42,56)	51(38,58)	44(39,56.5)	1.737	0.419
Sex					0.109	0.515
Male	76(45.0)	44(44.4)	12(48)	20(44.4)		
female	93(55.0)	55(55.6)	13(52)	25(55.6)		
Side					4.228	0.332
Lift	103(60.9)	61(61.6)	11(44)	31(68.9)		
right	66(39.1)	38(38.4)	14(56)	14(31.1)		
Diameter	2.10(1.60,2.60)	2.10(1.50,2.60)	2.00(1.70,2.65)	2.20(1.50,2.75)	0.224	0.894
CT-u	11.96±14.92	11.84±14.86	11.50±15.51	12.49±15.06	0.043	0.958
CT-u(max)	59.66±21.12	60.18±22.47	53.96±16.99	61.67±19.96	1.146	0.321
CT-u(min)	-37.91±23.25	-37.09 ± 21.08	-32.04 ± 22.88	-42.96 ± 27.24	1.938	0.147
Sev-u	15.9(12.90,18.96)	16.50(13.50,20.60)	14.70(13.20,17.05)	15.00(12.00,17.74)	5.994	0.05
CT-a	50.40(31.35,64.55)	51.00(29.50,64.30)	48.10(31.00,61.65)	47.00(32.50,69.50)	0.031	0.985
CT-a(max)	111.00(88.50,138.00)	114.00(88.00,138.00)	106.00(91.00,122.00)	113.00(89.50,142.50)	0.904	0.637
CT-a(min)	-14.85 ± 36.32	-15.12±29.34	-1.64 ± 36.12	-21.09 ± 47.60	0.098	0.121
Sev-a	20.90(17.00,24.27)	22.70(19.00,25.50)	19.20(16.00,22.00)	18.00(15.50,22.71)	16.312	< 0.001
CTa-CTu	35.70(25.60,50.85)	36.30(24.20,50.10)	39.20(25.80,49.55)	34.00(26.00,51.50)	0.154	0.926
CT-v	63.32±21.30	60.22 ± 20.00	62.10±16.39	69.00 ± 22.99	0.058	0.063
CT-v(max)	126.05 ± 26.77	123.53 ± 26.62	117.60±23.03	132.51 ± 26.95	2.998	0.166
CT-v(min)	0.00(-20.00,17.00)	-1.00(-16.00,15.00)	6.00(-3.50,24.00)	-12.00(-45.00,19.50)	5.805	0.055
Sev-v	20.30(17.45,24.25)	21.40(18.10,25.30)	20.00(15.40,22.70)	19.00(16.29,21.80)	11.922	0.003
CTv-CTu	50.00(41.95,58.25)	47.70(38.80,56.30)	48.50(42.50,56.80)	55.00(46.50,64.00)	9.626	0.008

Explanation: CTu: Average attenuation value in the unenhanced phase; CTu(max): Maximum attenuation value in the unenhanced phase; CTu(min): Minimum attenuation value in the unenhanced phase; CTu(min): Minimum attenuation value in the unenhanced phase; CTa: Average attenuation value in the arterial phase; CTa(max): Maximum attenuation value in the arterial phase; CTa(max): Maximum attenuation value in the arterial phase; CTa(max): Maximum attenuation value in the arterial phase; CTa(min): Minimum attenuation value in the arterial phase; CTa(max): Maximum attenuation value in the arterial phase; CTa(max): Maximum attenuation value in the arterial phase; CTa(min): Minimum attenuation value in the arterial phase; CTa-CTu: Difference between average attenuation values in the arterial phase; CTv(max): Maximum attenuation value in the venous phase; CTv(min): Minimum attenuation value in the venous phase; CTv-CTu: Difference between average attenuation values in the venous phase and the unenhanced phase; CTv-CTu: Difference between average attenuation values in the venous phase and the unenhanced phase; CTv-CTu: Difference between average attenuation values in the venous phase and the unenhanced phase; CTv-CTu: Difference between average attenuation values in the venous phase; Ar and for the Kruskal-Wallis H test, it is denoted as H

Table 3	Analysis of	clinical and ra	radiological features	in the three pati	ient categories within	the training set
	,					

	Training set				
	Total	APA	CPA	NAA	P-value
Sample size	99	39	27	33	
Sex					0.001
Male	44(44.4)	17(43.6)	5(18.5)	22(66.7)	
female	55(55.6)	22(56.4)	22(81.5)	11(33.3)	
age	51(42.00,56.00)	47.0 (36.00,54.00)	51.0 (38.00,55.00)	55.0 (48.50,58.50)	0.005
Side					0.566
Lift	61(61.6)	26(66.7)	17(63.0)	18(54.5)	
right	38(38.4)	13(33.3)	10(37.0)	15(45.5)	
Diameter	2.17±0.75	1.76±0.47	2.81±0.76	2.12±0.64	< 0.001
CTu	11.84±14.86	8.78±13.24	20.59 ± 13.40	8.29±15.25	0.001
CTu(max)	60.18±22.47	56.97 ± 23.90	69.85±18.83	56.06 ± 21.69	0.03
CTu(min)	-37.09 ± 21.08	-38.15±18.84	-26.96±18.79	-44.12±22.66	0.006
Sevu	16.50(13.50,20.60)	15.40(12.90,21.60)	16.10(13.40,19.70)	17.60(14.90,21.00)	0.476
СТа	48.96 ± 25.89	47.96±23.12	61.19±22.59	40.15 ± 28.23	0.006
CTa(max)	114.00(88.00.138.00)	111.00(93.00,121.00)	130.00(115.00,151.00)	96.00(80.00,136.00)	0.007
CTa(min)	-15.12 ± 29.34	-10.26 ± 26.72	-7.89 ± 26.56	-26.79±31.65	0.017
Seva	22.70(19.00,25.50)	22.60(17.60,25.30)	22.30(19.10,25.20)	23.20(20.00,26.85)	0.452
CTa-CTu	37.13±19.27	39.17 ± 20.58	40.60±17.70	31.87±18.32	0.151
CTv	60.22 ± 20.00	54.68 ± 15.30	73.87±19.76	55.61 ± 20.32	<0.001
CTv(max)	123.53±26.62	114.72±24.03	135.74±23.92	123.94 ± 28.28	0.006
CTv(min)	-2.93±26.63	-4.15±18.31	11.96±23.45	-13.67±31.93	0.001
Sevv	21.40(18.10,25.30)	20.30(17.60,25.30)	21.40(18.10,23.20)	23.30(20.25,25.75)	0.202
CTv-CTu	47.70(38.80,56.30)	44.70(37.00,50.30)	54.80(47.00,61.50)	45.50(39.75,55.10)	0.091

Explanation: NAA: non-functioning adrenal adenoma.CPA: Cortisol-producing adenoma. APA: Aldosterone-producing adenoma. CTu: Average attenuation value in the unenhanced phase; CTu(max): Maximum attenuation value in the unenhanced phase; CTu(min): Minimum attenuation value in the unenhanced phase; Sevu: Standard deviation of attenuation values in the unenhanced phase; CTa: Average attenuation value in the arterial phase; CTa(max): Maximum attenuation value in the arterial phase; CTa(min): Minimum attenuation value in the arterial phase; Seva: Standard deviation of attenuation values in the arterial phase; CTa-CTu: Difference between average attenuation values in the arterial phase; CTv(max): Maximum attenuation value in the venous phase; CTv(max): Maximum attenuation value in the venous phase; CTv(max): Maximum attenuation value in the venous phase; CTv(max): Difference between average attenuation values; In the venous phase; CTv-CTu: Difference between average attenuation values in the venous phase; CTv-CTu: Difference between average attenuation values; In the venous phase; CTv-CTu: Difference between average attenuation values; In the venous phase; CTv-CTu: Difference between average attenuation values in the venous phase; CTv-CTu: Difference between average attenuation values in the venous phase; CTv-CTu: Difference between average attenuation values in the venous phase; CTv-CTu: Difference between average attenuation values in the venous phase; CTv-CTu: Difference between average attenuation values in the venous phase; CTv-CTu: Difference between average attenuation values in the venous phase; CTv-CTu: Difference between average attenuation values in the venous phase; CTv-CTu: Difference between average attenuation values in the venous phase; CTv-CTu: Difference between average attenuation values in the venous phase; CTv-CTu: Difference between average attenuation values in the venous phase; CTv-CTu: Difference between average attenuation values in the venous phase; CTv-CTu: Difference between average at

each radiomics model, the aforementioned features were incorporated, leading to the selection of 102, 13, and 17 features for the unenhanced, arterial, and venous phases, respectively.

This procedure was repeated in a second round of selection. The final number of optimal features selected for the three phases were 13, 4, and 10, respectively. Results of the clinico-radiological features for the training set are shown in Table 3. Significant features (P < 0.05) were included in the final modeling. The results indicated that the triphasic model had the best performance among the radiomics models. The selected clinico-radiological features were combined with the triphasic radiomics features to establish a combination model. The optimal number, types, and weights of features for the six models are shown in Fig. 3.

Performance of the six models

The ROC curves and AUCs for the training and validation sets are presented in Fig. 4. Results of the sensitivity, specificity, precision, and accuracy values are listed in Table 4. The confusion matrices for the six models are illustrated in Fig. 5. AUC values for distinguishing APA from other adenomas, CPA from other adenomas, and NAA from other adenomas for the training and validation set were as follows: training set and validation set AUC were (0.95, 95% CI=0.90–0.99; 0.93, 95% CI=0.83–1.00); (0.96, 95% CI=0.93–1.00; 0.89, 95% CI=0.72–1.00); (0.94, 95% CI=0.90–0.98; 0.77, 95% CI=0.55–1.00), respectively. The results indicated that the combined model achieved the best predictive performance for APA and NAA, while the AUC for distinguishing CPA in the external validation set was relatively lower compared with that of the clinico-radiological model.

The AUC results for the external data are shown in Fig. 6. Notably, the AUCs of the joint model for distinguishing APA from other adenomas, CPA from other adenomas, and NAA from other adenomas were (0.86, 95% CI = 0.73–0.99), (0.89, 95% CI = 0.80–1.00), and (0.82, 95% CI = 0.68–0.95), respectively. External data further validated the results obtained from the internal data. The confusion matrix for the optimal model is presented in Fig. 7, and its sensitivity, specificity, precision, and accuracy are detailed in Table 4.



Fig. 3 The optimal feature types and feature weights of the unenhanced phase, arterial phase, venous phase, clinico-radiological, triphasic, and combine models

Discussion

In recent years, the incidence and detection rate of AI have been on the increase, with approximately 90% of cases being ACA. Among them, functional adenomas are a significant threat to patients' life and health, most of them requiring surgical intervention. However, most preoperative examination protocols are costly, cause significant trauma, and not sufficiently accurate, which limit their application in the preoperative diagnosis of adrenal tumors. Therefore, innovative preoperative diagnostic methods need to be developed to improve the diagnosis

of adrenal tumors. This study found that the combination models based on logistic regression can accurately predict the preoperative multi-classification of adrenal tumors, as evidenced by their performance in the external test set.

Previous studies have demonstrated radiomic models can effectively classify the diagnosis of adrenal tumors. For instance, Chen et al. [20] utilized CT radiomic models to differentiate non-functional adenomas from APA and to predict their prognosis. The results suggest that CT-based radiomic models are ideal for distinguishing



Fig. 4 ROC curves for classifying the prediction results of the three types of adrenal cortical adenomas in the internal training and validation sets. **a-c** The ROC curves for discriminating APA, CPA, and NAA in the four-phase models of the internal training set. **d-f** The ROC curves for discriminating APA, CPA, and NAA in the four-phase models of the internal training set. **d-f** The ROC curves for discriminating APA, CPA, and NAA in the four-phase models of the internal training set.

between APA and non-functional adenomas detected in CT imaging among hypertensive patients in clinical practice. Piskin et al. [21] developed a radiomics and clinical feature model using MRI data to differentiate between non-functional and autonomously secreting cortisol adrenal incidentalomas. They found that the radiomics models (OP, IP, IP plus T2-W model) showed superior performance in the training and testing datasets. Another study by Qi et al. [22] applied various radiomics classifiers to analyze functional and non-functional ACA. They reported that the radiomics model based on the logistic regression achieved the best performance.

However, most previous studies on adrenal radiomics did not include an external validation cohort and did not address the differential prediction of the models between two categories within the three classifications of adrenal adenomas. Moreover, the studies did not comprehensively evaluate the efficacy of any classifier model in accurately distinguishing between all three subtypes of adrenal adenomas. Furthermore, treatment strategies, preoperative preparation, and the timing of postoperative hormone replacement therapy vary significantly depending on the specific adenoma subtype. Therefore, a predictive model that can comprehensively predict all subtypes of adrenal adenomas needs to be developed. In addition, the three-class radiomics prediction model faces greater variability as the number of classifications increases. This increased complexity can decrease the model performance, presenting a significant challenge in enhancing the effectiveness of the model [23]. In this study, we validated the performance of the model in an external cohort, performed classification and differential prediction for all types of adrenal adenomas. The results indicated that the model could distinguish the three categories of adrenal adenomas with good generalizability. These findings may serve as a reference value for making treatment decisions and perioperative planning for patients.

Further analysis revealed that the three-class prediction model for adrenal adenomas outperformed or was comparable to that of previous studies in differentiating all three types of ACA [20–22, 24, 25]. Furthermore, we observed that the triphasic model exhibited the best performance among the radiomics models, which is in line with the findings of Qi et al. [22]. Moreover, we applied the same model to extract identical features within each imaging phase (unenhanced, arterial, and venous) for the purpose of differentiating between the three adenoma subtypes. Although this may potentially decrease the model efficacy, considering the universality and simplicity required for future clinical applications, our approach carries significant advantages.

This study demonstrated that in the combined model, age carried the greatest weight, including the inclusion of

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Classification	Model	Cohort	AUC(95% CI)	Sensitivity	Specificity	Accuracy	Precision
APA	Unenhance	Training set	0.91(0.85-0.97)	0.74	0.87	0.82	0.78
		Validation set	0.89(0.76-1.00)	0.70	0.87	0.80	0.78
		Test set	0.80(0.67-0.93)	0.60	0.83	0.64	0.76
	Arterial	Training set	0.83(0.75-0.91)	0.80	0.70	0.74	0.63
		Validation set	0.86(0.71-1.00)	0.90	0.67	0.76	0.64
		Test set	0.80(0.63-0.96)	0.73	0.57	0.46	0.62
	venous	Training set	0.87(0.80-0.94)	0.72	0.85	0.80	0.76
		Validation set	0.86(0.71-1.00)	0.60	0.87	0.76	0.75
		Test set	0.83(0.70-0.96)	0.73	0.83	0.80	0.67
	Triphasic	Training set	0.94(0.90-0.99)	0.85	0.93	0.90	0.89
		Validation set	0.93(0.84-1.00)	0.80	0.87	0.84	0.80
		Test set	0.86(0.73–0.99)	0.87	0.63	0.71	0.54
	Clinico-Radiological	Training set	0.84(0.76-0.92)	0.69	0.78	0.75	0.68
		Validation set	0.90 (0.77-1.00)	0.70	0.87	0.80	0.78
		Test set	0.80(0.64-0.97)	0.80	0.77	0.78	0.63
	Combine	Training set	0.95(0.90-0.99)	0.77	0.92	0.86	0.86
		Validation set	0.93(0.83-1.00)	0.70	0.80	0.76	0.70
		Test set	0.86(0.72-0.99)	0.80	0.70	0.73	0.57
CPA	unenhance	Training set	0.94(0.88-1.00)	0.89	0.86	0.87	0.71
		Validation set	0.79(0.58-1.00)	0.57	0.72	0.68	0.44
		Test set	0.69(0.52-0.86)	0.27	0.90	0.69	0.57
	arterial	Training set	0.86(0.74–0.95)	0.52	0.92	0.81	0.70
		Validation set	0.87(0.73-1.00)	0.57	0.94	0.84	0.80
		Test set	0.84(0.72-0.95)	0.33	0.87	0.69	0.56
	venous	Training set	0.91(0.85-0.97)	0.82	0.90	0.88	0.76
		Validation set	0.80(0.57-1.00)	0.71	0.72	0.72	0.50
		Test set	0.78(0.65-0.9)	0.80	0.60	0.67	0.50
	Triphasic	Training set	0.95(0.90-0.99)	0.82	0.92	0.89	0.79
		Validation set	0.83(0.64-1.00)	0.57	0.78	0.72	0.50
		Test set	0.81(0.68-0.94)	0.53	0.90	0.78	0.73
	Clinico-Radiological	Training set	0.88(0.80-0.96)	0.74	0.94	0.89	0.83
		Validation set	0.93(0.81-1.00)	0.57	0.94	0.84	0.80
		Test set	0.87(0.76-0.99)	0.73	0.97	0.89	0.92
	Combine	Training set	0.96(0.93-1.00)	0.85	0.90	0.89	0.77
		Validation set	0.89(0.72-1.00)	0.71	0.83	0.80	0.63
		Test set	0.89(0.77-1.00)	0.60	0.93	0.82	0.82

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Table 4 (continued)

Classification	Model	Cohort	AUC(95% CI)	Sensitivity	Specificity	Accuracy	Precision
NAA	unenhance	Training set	0.87(0.80-0.94)	0.58	0.86	0.77	0.68
		Validation set	0.62(0.38-0.86)	0.38	0.77	0.64	0.43
		Test set	0.60(0.43-0.77)	0.27	0.77	0.60	0.63
	arterial	Training set	0.73(0.62-0.83)	0.46	0.77	0.67	0.50
		Validation set	0.74(0.52-0.97)	0.50	0.88	0.76	0.67
		Test set	0.78(0.64-0.93)	0.27	0.87	0.67	0.50
	venous	Training set	0.81(0.72-0.91)	0.61	0.80	0.74	0.61
		Validation set	0.63(0.41-0.86)	0.25	0.71	0.56	0.29
		Test set	0.71(0.55–0.87)	0.20	0.93	0.69	0.60
	Triphasic	Training set	0.91(0.85–0.97)	0.79	0.88	0.85	0.77
		Validation set	0.72(0.50-0.95)	0.50	0.82	0.72	0.57
		Test set	0.74(0.58-0.90)	0.47	0.90	0.76	0.70
	Clinico-Radiological	Training set	0.79(0.70-0.88)	0.64	0.79	0.74	0.60
		Validation set	0.65(0.40-0.89)	0.63	0.65	0.64	0.46
		Test set	0.80(0.65-0.94)	0.60	0.83	0.76	0.64
	Combine	Training set	0.94(0.90-0.98)	0.82	0.89	0.87	0.79
		Validation set	0.76(0.55–0.98)	0.50	0.82	0.72	0.57
		Test set	0.82(0.68-0.95)	0.60	0.87	0.78	0.69

Explanation: NAA: non-functioning adrenal adenoma. CPA: Cortisol-producing adenoma. APA: Aldosterone-producing adenoma

sex and tumor size. This is consistent with the findings by Oksana et al. [26], who suggested that these features are associated with the adrenal ACA subtypes. Cristina et al. [8] uncovered that the tumor diameter and mean attenuation value in the venous phase can effectively distinguish CPA. In contrast, Chan et al. [27] reported that tumor size, mean attenuation value in the unenhanced phase, and mean attenuation value in the enhanced phase can facilitate the differentiation of CPA. Among the radiomics features, the 10th percentile and Gray-Level Co-occurrence Matrix (GLCM) features exerted significant weights and proportions. The Gray-Level Cooccurrence Matrix (GLCM), as a classical texture analysis method, reveals the spatial distribution and variability of image textures by statistically analyzing the distribution of gray levels in adjacent pixel pairs. This feature descriptor plays an important role in tasks such as tumor segmentation, lesion detection, and tissue classification in the field of image processing. Percentiles, as an intuitive statistical measure, describe the value corresponding to a specific percentage of data points within a dataset. This value represents the gray level below which 10% of the pixels in an image fall, indicating the distribution of low-intensity regions within the image. Previous studies [28] have suggested that APA contained clear cells or dense eosinophilic cells or a combination of both. On the contrary, CPA consists of enlarged "balloon-like" cells with increased lipid accumulation in the cytoplasm. The Grey level co-occurrence matrix feature generally indicates grayscale relationships between pixels in image maps, reflecting tissue structure and complexity, which is closely associated with the cellular composition of the

aforementioned tumors. Chan et al. [27] demonstrated that CPA may manifest as relatively large and high-density masses on CT scans, while APA may appear as relatively small and low-density masses. The 10 percentile typically reflects the distribution of grayscale and brightness pixels in image maps, and in CT images, grayscale and brightness reflect tumor density. In the statistical analysis of tumor maximum diameter, our results were consistent with those of the aforementioned studies. Moreover, others scholars [27, 29] found that the pathological morphology of APA and non-functioning adrenal ACA are similar. However, the CT manifestations of functional and non-functional adenomas may exhibit significant overlap. Therefore, this may explain the relatively lower discriminatory performance of the model in identifying NAA.

This study has several limitations: (1) Although we performed external validation, the results obtained may be limited by the small sample size and retrospective nature of the study. Future research should involve larger sample sizes, multicenter studies, and prospective designs to validate the present findings. (2) Some patients did not undergo gold-standard diagnostic tests due to various constraints and patient preferences. Consequently, we included as many classification criteria as possible, which led to the exclusion of many patients. However, the occurrence of false-negative results remains unavoidable. (3) This study utilized a single classifier model for validation. Future research should perform model training and exploration of more models to achieve optimal prediction results. (4) In the present study, we included only adrenal tumors with a diameter exceeding 1 cm, consistent with



Fig. 5 Confusion matrix based on internal data training and validation results



Fig. 6 ROC curves of classification prediction results for the three types of adrenal cortical adenomas in the external test set. **a-c** The ROC curves for discriminating APA, CPA, and NAA in the four-phase models of the internal training set



Fig. 7 Confusion matrix based on external data test results

the commonly accepted definition of adrenal incidentalomas. Therefore, further research may be necessary to investigate tumors smaller than 1 cm.

Conclusion

The logistic regression classifier model, incorporating both clinico-radiological and radiomic features, proves to be effective in distinguishing adrenal adenoma subtypes. As a non-invasive preoperative diagnostic tool, it holds substantial promise for future clinical applications.

Abbreviations

Adrenocortical adenomas
Adrenal incidentaloma
Aldosterone-producing adenoma
Aldosterone/renin ratio
Area under the curve
Cortisol-producing adenoma
Gray-LevelCo-occurrence Matrix
Inter-correlation coefficient
Non-functioning adrenal adenoma
Picture archiving and communication system
Recursive Feature Elimination with Cross-Validation
Receiver operating characteristic curve

Supplementary Information

The online version contains supplementary material available at https://doi.or g/10.1186/s12880-025-01556-w.

Supplementary Material 1

Acknowledgements

The extraction of radiomics features and the establishment of the radiomics model were supported by the Darwin Research Platform.

Author contributions

All authors contributed to the conception, design, and supervision of the project. LW and WJF led and coordinated the study. SYP and HPP collected data from Center 1; SX and YML collected data from Center 2. LJJ annotated the CT images, and YML and LW carefully reviewed the annotated data. Clinical data review and statistical analysis were performed by ZYW and ZY. With suggestions and research services for feature engineering and model design provided by LH and CJQ. ZXZ and YLY preprocessed all the data, analyzed the image features, and constructed the radiomics model. ZXZ and SYP were the main contributors to manuscript writing. YJF provided constructive suggestions for the study. SW, ZJP, and LWL provided significant assistance in revising the manuscript. All authors have reviewed, edited, and approved the final version of the manuscript.

Funding

This work was supported by the Medical leading talents Project in Yunnan Province (grant numbers L-2019016) and the Yunnan Province High-level personnel training support Program famousMedical Project (grant numbers YNWR-MY-2020-035).

Data availability

The datasets used and/or analysed during the current study are available from the corresponding author on reasonable request.

Declarations

Ethics approval and consent to participate

This study is a retrospective study and has been approved by the Medical Ethics Committee of the First People's Hospital of Yunnan Province (No. KHLL2023-KY170) and the Second Affiliated Hospital of Kunming Medical University (No. 2023 - 233). Due to retrospective and anonymous analysis, the ethics committee waived the requirement for informed consent.

Consent for publication

Not applicable.

Clinical trial number

Not applicable.

Competing interests

The authors declare no competing interests.

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Received: 1 November 2024 / Accepted: 8 January 2025 Published online: 10 February 2025

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