

## Monitoring Tissue-Engineered Graft Oxygenation *In Vivo* by Fluorine-19 Magnetic Resonance Spectroscopy

Samuel A Stein<sup>1</sup>, Bradley P Weegman<sup>1</sup>, Thomas M Suszynski<sup>2</sup>, Meri T Firpo<sup>3</sup>, Melanie L Graham<sup>2</sup>, Klearchos K Papas<sup>4</sup>, and Michael Garwood<sup>1</sup>

<sup>1</sup>Radiology, University of Minnesota, Minneapolis, MN, United States, <sup>2</sup>Surgery, University of Minnesota, Minneapolis, MN, United States, <sup>3</sup>Medicine, University of Minnesota, Minneapolis, MN, United States, <sup>4</sup>Surgery, University of Arizona, Tucson, AZ, United States

**Purpose:** Transplantation of tissue-engineered grafts (TEGs) has the potential to treat numerous debilitating diseases. Non-invasive monitoring of the oxygen partial pressure ( $pO_2$ ) in TEGs is critically important because of the harmful effects of prolonged or even short-term exposure to hypoxia and anoxia. This monitoring is particularly important in the early post-transplant period (before revascularization) or if a TEG is immunoisolated (and does not revascularize). Additionally, *in vivo* tissue  $pO_2$  measurements may enable detection of events that would alter oxygenation of a TEG such as fibrous capsule formation, vascularization, inflammation, or cell proliferation, as well as the estimation of cell or tissue viability<sup>1</sup>. The spin relaxation mechanisms of some biocompatible fluorine compounds are very sensitive to dissolved oxygen (and temperature) and insensitive to other external factors<sup>2</sup>. Fluorine-19 nuclear magnetic resonance spectroscopy (19F-MRS) can, therefore, be used to quantify the oxygenation status of a TEG. This pilot study evaluated the utility of 19F-MRS for the non-invasive measurement of *in vivo*  $pO_2$  within macroencapsulated TEGs following implantation in the murine model.

**Methods:** TEGs were constructed by injecting an emulsion of perfluoro-15-crown-5-ether (PFCE) and porcine plasma into a 40- $\mu$ L TheraCyte® immunoisolation device (TheraCyte, Inc. Laguna Hills, CA), which was then crosslinked using 5% v/v bovine thrombin solution. An image of the encapsulation device and the distribution of fluorine in the device are shown in Figure 1. A linear correlation between the spin-lattice relaxation rate ( $R_1$ ) and oxygen concentration was established before implantation of a TEG (Figure 2), and this correlation was used to convert measurements of  $R_1$  to local  $pO_2$  within the TEG following implantation. Nine male Lewis rats were implanted with a TEG into a dorsal subcutaneous pocket and assigned to groups for serial evaluation of oxygen content in relation to implant day +1 (n=3), +8 (n=3), and +15 (n=3). On the day of evaluation, rats were anesthetized with inhalation isoflurane, stabilized at a core body temperature of 37 °C, and imaged using a 16.4 T horizontal-bore magnet (Agilent Technologies Santa Clara, CA). Then, 19F-MRS was performed using a single-loop surface coil and an inversion-recovery sequence was used to obtain the  $R_1$  from the singlet PFCE resonance within the TEGs.  $R_1$  measurements within the TEG were then converted to  $pO_2$  values using the linear calibration. Following imaging, animals were promptly euthanized using CO<sub>2</sub> for device explant and gross evaluation.

**Results:** The mean  $pO_2$  in the encapsulated TEG 1 day post-implantation was 69±22 mm Hg. The mean  $pO_2$  fell over time to 16±3 mm Hg at 8 days post-implantation and 0±10 mm Hg at 15 days post-implantation (Figure 3).

**Conclusion:** These preliminary studies confirm that 19F-MRS can be used to non-invasively measure  $pO_2$  *in vivo* within a macroencapsulated TEG. Preliminary data suggest that the encapsulated TEG becomes hypoxic 1 week post-implantation despite the oxygen permeable membrane and may require supplemental oxygenation to sustain cells and tissue. Future studies will attempt to correlate  $pO_2$  measurements with changes in TEG viability and oxygenation both pre- and post-transplantation.

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### References:

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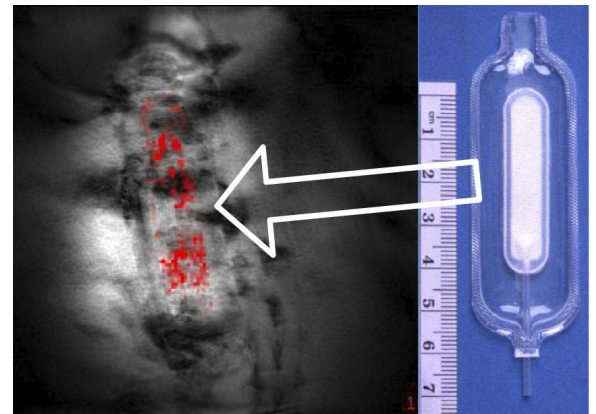


Figure 1: A photograph of the encapsulation device in sterile packaging and a 19F/1H fusion MRI showing the distribution of fluorine in the device implanted in a rat.

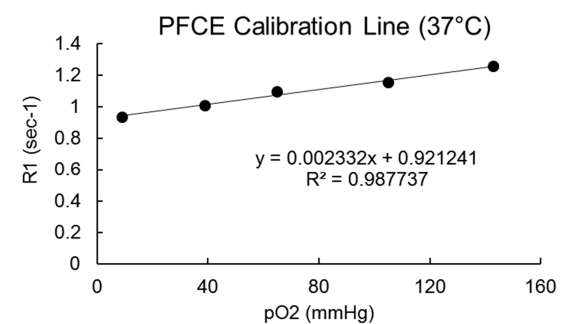


Figure 2:  $R_1$  was confirmed to be linear with  $pO_2$  at 37 °C. This relationship was used to quantify the oxygen status of the TEGs.

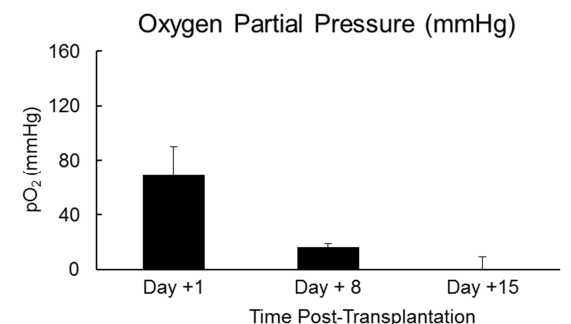


Figure 3: The results of the *in vivo* experiments. While initially at room oxygen (160 mm Hg), after implantation the TEGs quickly become hypoxic. They are measured to be anoxic two weeks post-implantation.