## Supplementary Information

## **Supplementary Table 1.** Related work.

Work	Year	# P	atients	Sym	ptoms	Sensors	# Devices	Locations	Data Collection	Criterion Validity	Discriminative Validity	Utility	Algorithm
		PD	Controls	Tremor	Brady- kinesia								
Hoff et al.	2004	15		Yes	Yes	Accelerometer	3	Sternum, wrist and thigh on most affected side	24 hour recording Motor diaries	No	Yes	No	Heuristic algorithm based on empirically derived thresholds.
Keijsers et al.	2006	23		Yes	Yes	Accelerometer	6	Both upper arms and upper legs, sternum, wrist on most affected side	35 ADLs ~3hr monitoring period (ON/OFF)	No	Yes	No	Heuristic algorithm based on empirically derived thresholds.
Salarian et al.	2007	21	10	Yes	Yes	Gyroscope	2	Both wrists	15 ADLs + alternating hand movement (right and left)	Yes	Yes	No	Heuristic algorithm based on empirically derived thresholds.
Zwartjes et al.	2010	6	7	Yes	Yes	Accelerometer Gyroscope	4	Sternum, wrist, thigh and foot on the most affected side	8 ADLs + 5 motor assessment tasks	Yes	Yes	No	Heuristic algorithm based on empirically derived thresholds.
Griffiths et al.	2012	34	10	No	Yes	Accelerometer	1	Wrist on the most affected side	ADLs and constrained motor tasks in lab Upto 10 days at home	Yes	No	No	Proprietary. Heuristic algorithm based on empirically derived thresholds.

Rigas et al.	2012	18	5	Yes	No	Accelerometer	6	Both wrists and ankles, sternum, waist	5 ADLs + 3 motor assessment tasks	Yes	No	No	Posture recognition and tremor severity estimation algorithm trained using machine learning (HMM).
Roy et al.	2013	19	4	Yes	No	Accelerometer EMG	4	Both forearms and shanks	Self selected ADLs	Yes	No	No	Symptom detection algorithm trained using machine learning (DNN). MAP classifier for estimating severity of symptoms.
Tzallas et al.	2014	24(in lab) 12 (at home)	5	Yes	Yes	Accelerometer Gyroscope	5	Both wrists and ankles, waist	Prescribed and self- selected ADLs In lab: ~15 minutes/subj ect At home: ~8 hours/subjec t	Yes	No	Yes	Machine learning classifiers for assessment of tremor, bradykinesia and dyskinesia
Horne et al.	2015	64	38	No	Yes	Accelerometer	1	Wrist on the most affected side	Upto 10 days at home	Yes	Yes	No	Proprietary. Heuristic algorithm based on empirically derived thresholds (Griffiths et al. 2012).

Braybrook et al.	2016	194	28	Yes	No	Accelerometer	1	Wrist on the most affected side		No	Yes	No	Heuristic algorithm based on empirically derived thresholds.
Pulliam et al.	2018	13		Yes	Yes	Accelerometer Gyroscope	2	Wrist and ankle on the most affected side	6 ADLs (hygiene, eating, dressing, desk work, entertainme nt, laundry) ON/OFF	No	Yes	No	Proprietary. Heuristic algorithm based on empirically derived thresholds.
Rodríguez- Molinero et al.									1 - 3 days at home Motor				Machine learning classifier for gait detection. Heuristic algorithm for bradykinesia assessment based on movement fluidity during gait using patient specific
	2018	23		No	Yes	Accelerometer	1	Waist	diaries	No	Yes	No	threshold.

Scripted MDS-UPDRS-III Activities	Activities of Daily Living	Controlled Speech Activities
(3.3) Rigidity (neck, wrist/elbow and hip/knee)	(1) Tying a shoe	(1) Conversation. Subject discusses things that excite him or her.
(3.4) Finger tapping (right and left)	(2) Writing a sentence	(2) Picture description. Subject discusses everything he or she sees in a provided picture.
(3.5) Hand movements (flexion/extension)	(3) Writing cursive	(3) Reverse counting. Subject counts backwards from 405 to 375 by 3's.
(3.6) Pronation-supination movements of hand	(4) Fold a piece of paper	(4) Reading. Subject reads an excerpt from a book.
(3.7) Toe tapping	(5) Put on and remove jewelry	(5) Syllables. Subject repeats the word 'PATAKA' as many times as they can in 10 seconds.
(3.8) Leg agility	(6) Use a remote control (press 507, 169, 746)	
(3.9) Arising from chair (arms crossed and fast)	(7) Shake a bottle 5x, open bottle, drink, and close	
(3.10) Gait: 2.5m and 10m	(8) Pour a cup of water, take a drink, return cup to table, take another drink	
(3.12) Postural stability	(9) Eat with a spoon 2x	
(3.13) Posture (eyes open/closed)	(10) Take a lab coat off a hook/table, put it on, button all the buttons, then unbutton all the buttons, take off the lab coat and place back on hook/table	
(3.15) Postural tremor of the hands	(11) Take a sweatshirt off a hook/table, put it on, zip up the zipper, then unzip the sweatshirt, take off the sweatshirt and place back on hook/table	

**Supplementary Table 2.** List of activities performed in both PD and HC studies.

(3.16) Kinetic tremor of the hands (finger to nose)	(12) Open and close a door	
(3.17) Rest tremor	(13) Carry a book out and back 10m and place on table	
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	<ul><li>(14) Carry a suitcase out and back</li><li>10m, then hold suitcase for 90</li><li>seconds with forearm at 90</li></ul>	
	degrees.	

**Supplementary Table 3.** Features extracted for training the tremor and gait classifiers. For each classifier, a checkmark ( $\checkmark$ ) indicates that the feature was extracted and an asterisk (\*) indicates that the feature survived after the feature selection step.

Feature	Description	<b>Tremor Classifier</b>	Gait Classifier
Root mean square value	Root mean square value of a sensor data in a given time window. The RMS value is a measure of signal energy. Value of signal energy feature for accelerometer data is correlated with amount and intensity of motion.	√*	√*
Signal range	Range of signal values. Signal range provides a measure of the extremes of motion observed in a given time window of sensor data. Higher range would indicate occurrence of a large excursion in sensor values.	√*	√*
Signal entropy	Signal entropy is calculated by estimating Shannon entropy of the probability mass function of a signal <sup>32</sup> . Signal entropy values close to zero indicate that the signal is periodic and smooth, whereas large negative values indicate that the signal is irregular and non-periodic.	√*	√*
Correlation coefficient	Cross-correlation coefficient of data from 2 sensor streams (e.g. X axis and Y axis). The cross-correlation coefficient captures degree of co- ordination in the motion between orthogonal directions. Higher values		√*

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	indicate synchronous changes		
	occurring between the two		
	input signals.		
IQR of auto-covariance	Interquartile range of auto-		$\checkmark$
	covariance is a measure of		
	long-range dependency or		
	periodicity of a signal. Range		
	of auto-covariance captures if		
	the signal is periodic or		
	irregular.		
Mean cross rate	Number of times signal		√*
	changed from positive to		
	negative normalized by total		
	signal length.		
Range count percentage	Counts of observed time		$\checkmark$
	signal is between a given		
	range (percentage).		
Dominant frequency	Value of the frequency with	√*	√*
	the highest magnitude in the		
	normalized power spectrum		
	of the accelerometer signal.		
	Dominant frequency value		
	captures the fundamental		
	frequency of the underlying		
	movement (e.g. tremor,		
	walking) producing the		
	acceleration signal.		
Dominant frequency	Magnitude of the dominant	√	√*
magnitude	frequency in the normalized		
0	power spectrum. This feature		
	captures the percentage of		
	total signal energy in the		
	dominant frequency. High		
	values indicate that most of		
	the signal energy is		
	concentrated in the dominant		
	frequency and low values		
	indicate the signal energy is		
	maleute the signal energy is	1	

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	spread across the different		
	frequencies in the power		
	spectrum.		
Ratio of dominant frequency	Ratio of the energy in the	$\checkmark$	$\checkmark$
band to total energy in	dominant frequency		
spectrum	component to the sum of		
1	energy in the entire frequency		
	spectrum of a signal. This		
	feature captures periodicity of		
	a signal by calculating the		
	ratio of the energy in the		
	dominant frequency		
	component to the sum of		
	energy in the entire frequency		
	spectrum of a signal.		
Spectral flatness	Spectral flatness is calculated	√*	√*
	by dividing the geometric		
	mean of the power spectrum		
	with the arithmetic mean.		
	Spectral flatness captures the		
	amount of modulation or the		
	level of consistency and		
	ranges from 0 to 1.		
Spectral entropy <sup>33</sup>	Spectral entropy is calculated	√*	√*
1 15	by estimating Shannon	•	
	entropy of the probability		
	mass function of the power		
	spectrum of a signal. Values		
	closer to 1 indicate presence		
	of white noise. Values closer		
	to 0 indicate presence of		
	periodicity in the signal.		