Supplementary Note 1

A feature-based approach has low discriminatory power for the detection of AF

For a baseline comparison, we investigate the effectiveness of a traditional feature-based machine learning method against our model. Baseline results are reported in Table 1. Nine features most commonly used in feature-based AF detection and signal quality estimation algorithms9–11 were calculated for input into a MultiOutputClassifier random forest model from scikit-learn40. DeepBeat substantially outperforms the trained random forest model for AF detection across all metrics considered. The random forest results were dramatically less effective for detecting AF events compared to DeepBeat's AF event metrics. Our model's notable improvement in AF detection over other feature-based methods is reflective across all DeepBeat versions examined, demonstrating that a feature-based approach fails to have high discriminatory power for AF detection.

Details regarding random forest

To investigate the choice of a multi-task model, a comparison of different methods was performed. For a feature-based approach, random forests were used due to its capability of finding complex nonlinear relationships in data. The following features were calculated: kurtosis, skew, entropy, zero crossings, hjorthe mobility, hjorthe complexity, normalized root mean of successive differences, and Shannon entropy. A MultiOutputClassifier random forest model with n_estimators=100 and random_state=1 was used as parameters for training.

Supplementary Note 2

Details regarding 1D VGG

To investigate the choice of deep learning models, we selected the popular VGG12 architecture and adapted it for 1D input. Details of specifics regarding model architecture can be found in Table S6. Training of 1D VGG was similar to the approach used for DeepBeat, weights were randomly initiated according to He distribution 31 and hyperas was used for optimal selection of epoch, batch size and learning rates.

Supplementary Note 3

Results from unsupervised pre-training using convolutional denoising autoencoders

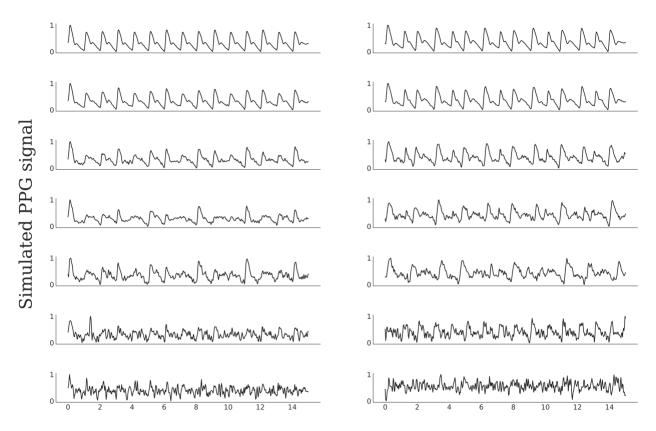
Results from the trained CDAE on scored signal quality assessment dataset can be found in supplemental Table S2. The mean squared errors were 0.0095, 0.0104, 0.0.0143 for excellent, acceptable and poor categories for the 25 second time segments. We found the lowest mean squared error for signal reconstruction in the excellent category across all time segments, suggesting that the trained CDAE is selecting filters appropriate for high-quality physiological signal reconstruction.

In order to determine that the CDAE was not introducing modulations typical of physiological signals when there was no physiological signal present, we performed a sensitivity analysis. Five hundred random signals were generated and ran through the trained CDAE model. The estimated MSE of the randomly generated noise was similar to that of the estimated MSE for the poor signal quality category across all time points. To further explore the estimated reconstruction predictions from the output of the trained CDAE, predictions were compared to

3rd order Savitzky-Golay filters. Mean squared error of the reconstruction CDAE prediction of the randomly generated noise set was 0.026, and the mean squared error of the 3rd order Savitzky-Golay filters was 0.023. These results confirm that the trained CDAE model provides a set of filters sensitive to frequencies unique to physiological signals and, in situations where no viable physiological signal is present, CDAE instead acts as a smoothing filter (Supplementary Figure 2).

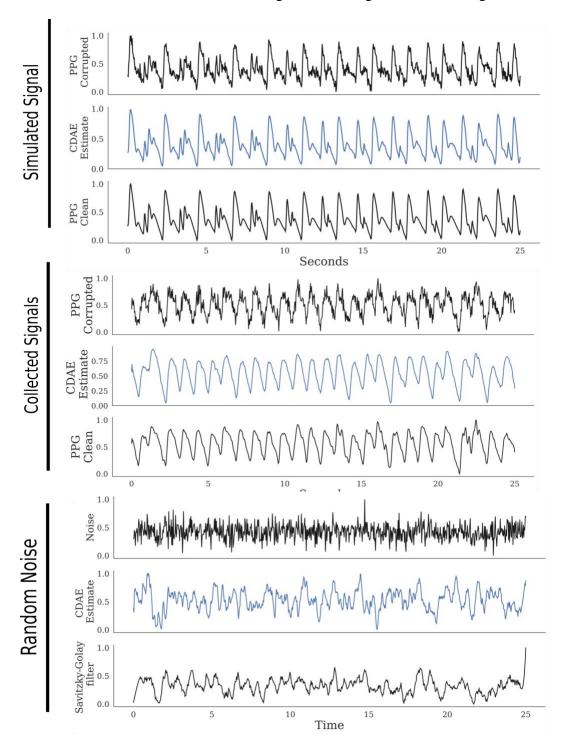
Supplementary Figure 1

Simulated signals from dataset A. Left column, simulated sinus rhythm, top to bottom in increasing order of added Gaussian noise mixture (0.001, 0.15, 0.5, 0.75, 1, 2, 5). Right column, simulated AF rhythm, top to bottom in increasing Gaussian noise mixture (0.001, 0.15, 0.5, 0.75, 1, 2, 5). Pictured below all signals were simulated at 60 beats per minute (BPM).



Time (secs)

Supplementary Figure 2
Results from trained CDAE on denoising simulated signals, collected signal and random noise.



Supplementary Table 1Breakdown of data samples by rhythm and quality assessment

partition	rhythm	QA	Count
		poor	999,253
	sinus	acceptable	140,020
train		excellent	390,851
		poor	972,955
	AF	acceptable	141,004
		excellent	159,851
		poor	295,449
	sinus	acceptable	56,572
validate		excellent	119,154
		poor	33,691
	AF	acceptable	8,075
		excellent	5,841
		poor	8,856
test	sinus	acceptable	1,718
		excellent	2,813
		poor	3,483
	AF	acceptable	314
		excellent	433

Supplementary Table 2
Comparison of evaluation data sets

	Number of patients	Total number of windows	Total number of AF windows
Held out test set	22	17,617	4,230
Ambulatory cohort	15	20,492	2,048

Supplementary Table 3

CDAE model architecture specifications

Layer Type	Output Shape	Param #			
Encoder					
InputLayer	(None, 800, 1)	0			
Conv1D	(None, 800, 64)	704			
MaxPooling	(None, 266, 64)	0			
Conv1D	(None, 266, 45)	23,085			
MaxPooling	(None, 88, 45)	0			
Conv1D	(None, 88, 50)	11,300			
MaxPooling	(None, 44, 50)	0			
	Decoder				
Conv1D	(None, 44, 50)	12,550			
UpSampling	(None, 88, 50)	0			
Conv1D	(None, 88, 45)	18,045			
UpSampling	(None, 264, 45)	0			
Conv1D	(None, 264, 64)	28,864			
UpSampling	(None, 792, 64)	0			
Flatten	(None, 50688)	0			
Dense	(None, 800)	40,551,200			

Supplementary Table 4

CDAE mean squared error for signal reconstruction

	Excellent	Acceptable	Poor
25 seconds	0.0095	0.0104	0.0143

Supplementary Table 5
DeepBeat model architecture specifications

			Layer Type	Output Shape	Param #			
			N 222	cted Encoder				
			InputLayer	(None, 800, 1)	0	1		
			Conv1D	(None, 800, 64)	704			
			MaxPooling	(None, 266, 64)	0			
			Conv1D	(None, 266, 45)	23,085			
			MaxPooling	(None, 88, 45)	0			
			Conv1D	(None, 88, 50)	11,300			
			MaxPooling	(None, 44, 50)	0			
			Sh	ared layers		1		
			BatchNormalization	(None, 44, 50)	200	1		
			Conv1D	(None, 15, 64)	12864			
			Leaky ReLu	(None, 15, 64)	0			
			BatchNormalization	(None, 15, 64)	256			
			Dropout	(None, 15, 64)	0			
			Conv1D	(None, 5, 35)	8995			
			Leaky ReLu	(None, 5, 35)	0			
			BatchNormalization	(None, 5, 35)	140			
			Dropout	(None, 5, 35)	0			
			Conv1D	(None, 5, 64)	9024			
			Leaky ReLu	(None, 5, 64)	0			
			BatchNormalization	(None, 5, 64)	256			
Rhythm Branch			Dropout	(None, 5, 64)	0	Quality Assessment Branch		
Conv1D	(None, 2, 35)	11235				Conv1D	(None, 3, 25)	6425
BatchNormalization	(None, 2, 35)	140				BatchNormalization	(None, 3, 25)	100
Dropout	(None, 2, 35)	0				Dropout	(None, 3, 25)	0
Conv1D	(None, 1, 25)	525				Flatten	(None, 75)	0
BatchNormalization	(None, 1, 25)	100				Dense	(None, 175)	13300
Dropout	(None, 1, 25)					Dense	(None, 3)	528
Conv1D	(None, 1, 35)	2660						
BatchNormalization	(None, 1, 35)	140						
Dropout	(None, 1, 35)	0						
Flatten	(None, 35)	0						
Dense	(None, 175)	6300						
Dense	(None, 2)	352						